

Real-time 3D Segmentation of the Left Ventricle Using Deformable Subdivision Surfaces F. Orderud¹ and S.I. Rabben² ¹ Norwegian University of Science and Technology (NTNU), Trondheim, Norway, ² GE Vingmed Ultrasound, Oslo, Norway

Deformable Subdivision Surface

- Use method of J. Stam to evaluate arbitrary Doo-Sabin subdivision surface. points on subdivision surface:
- Subdivide mesh recursively until desired point lies within a regular surface patch.
- Implement subdivision analytically, as a matrix exponential operation.
- Precalculate basis functions for surface points during tracking initialization.
- Surface point evaluation can then be performed efficiently (weighted sum).



- Generalizes bi-quadric B-splines to arbitrary topology.
- Control vertices move during tracking to alter shape.
- Global transform to position, scale and orient the model.



Tracking framework

- State-estimation approach to 3D segmentation.
- State vector consisting of control vertex positions (x) and global transform parameters (**x**_q):

$$\mathbf{x} \equiv \left[\mathbf{x}_g^T, \mathbf{x}_l^T\right]^T$$

- Use an extended Kalman filter for state estimation:
- 1) Kinematic model to predict state vector for each new frame:

 $\bar{\mathbf{x}}_{k+1} - \mathbf{x}_0 = \mathbf{A}_1(\mathbf{\hat{x}}_k - \mathbf{x}_0) + \mathbf{A}_2(\mathbf{\hat{x}}_{k-1})$

- 2) Create a model based on the prediction, and compute surface points.
- Compute Jacobian matrices (**J**) for each surface point.
- 3) Perform edge-detection along surface normals.
- Compute normal displacement (v), measurement variance (*r*) and a measurement vector (**h**) for each edge:

$$v = \mathbf{n}^T (\mathbf{p}_{obs} - \mathbf{p}) \qquad \mathbf{h}^T = \mathbf{n}$$

(b) Two views of a fitted subdivison surface, showing red surface patches and control vertices in the encapsulating wire-frame

Edge-detection

- rejection.





Block diagram over the separate stages in the tracking framework

- Measurement update:
 - Assume independent measurements.
 - Perform outlier removal for edge measurements.
- 4) Assimilate edge-detection measurements in information space:

$$\mathbf{H}^T \mathbf{R}^{-1} \mathbf{v} = \sum_i \mathbf{h}_i r_i^{-1} \mathbf{v}$$
$$\mathbf{H}^T \mathbf{R}^{-1} \mathbf{H} = \sum_i \mathbf{h}_i r_i^{-1} \mathbf{h}_i$$

5) Fuse measurements with the prediction to compute an updated state estimate:

$$\hat{\mathbf{x}}_{k} = \bar{\mathbf{x}}_{k} + \hat{\mathbf{P}}_{k} \mathbf{H}^{T} \mathbf{R}^{-1} \mathbf{v}_{k}$$
$$\hat{\mathbf{P}}_{k}^{-1} = \bar{\mathbf{P}}_{k}^{-1} + \mathbf{H}^{T} \mathbf{R}^{-1} \mathbf{H}$$

$$- x_0)$$

Example Screenshot



Screenshot from real-time 3D segmentation in 3D echocardiography

Results

- From 21 unselected 3D echocardiography recordings (GE Vivid 7 scanner).
- Tracking initialized by placing the model in the center of the image volume.
- Successful segmentation in all 21 recordings.
- Segmented meshes were compared to meshes from a semi-automatic segmentation tool (GE Vingmed):

Distance [mm] EDV [ml] ESV [ml] EF [%] 3.6 ± 21.4 9.0 ± 17.4 -5.9 ± 11.1 2.2 ± 0.8 Table 1. Bland-Altman analysis of the segmentation results com- Figure 4. Volume correlation plot for the proposed segmentapared to the reference segmentation. Results are expressed as tion against the reference method at end-diastole (EDV) and endsystole (ESV) in each of the 21 recording. mean difference ± 1.96 SD.

Bland-Altman analysis of mesh distances and volume correspondence

Conclusion

- Real-time 3D segmentation with subdivision surfaces in dense volumetric data is computationally feasible.
- Using a Kalman filter, tracking of the left ventricle can be performed fully automatic, and in real-time.







 25fps segmentation consumes 8% CPU on a 2.16GHz dual-core CPU!

